



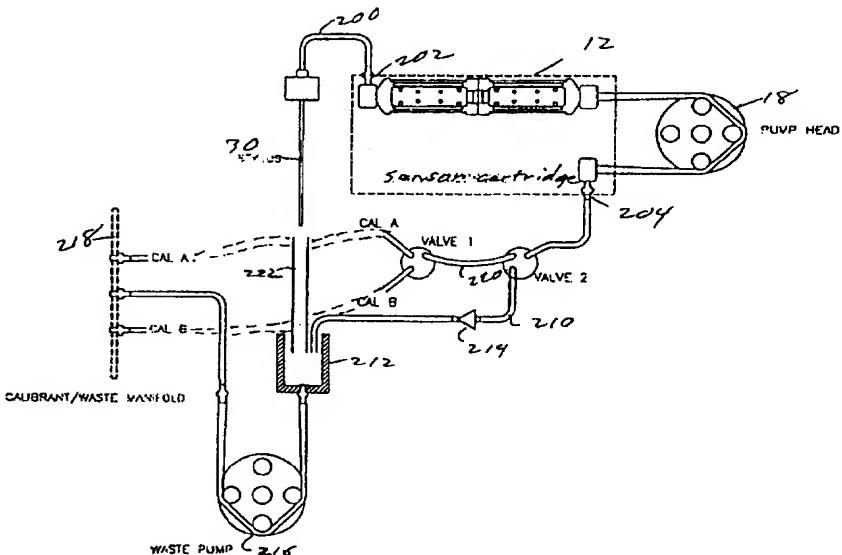
INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification ⁶ : G01N 35/10	A1	(11) International Publication Number: WO 97/44672 (43) International Publication Date: 27 November 1997 (27.11.97)
(21) International Application Number: PCT/US97/08737		(81) Designated States: AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, DE, DK, EE, ES, FI, GB, GE, HU, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, TJ, TM, TR, TT, UA, UG, UZ, VN, ARIPO patent (GH, KE, LS, MW, SD, SZ, UG), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG).
(22) International Filing Date: 20 May 1997 (20.05.97)		
(30) Priority Data: 08/650,341 20 May 1996 (20.05.96) US		
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(54) Title: PORTABLE MODULAR BLOOD ANALYZER WITH SIMPLIFIED FLUID HANDLING SEQUENCE

(57) Abstract

A portable, modular blood analyzer capable of analyzing multiple blood values in an inexpensive, relatively simple, easy-to-use and easy-to-maintain instrument. The invention comprises a three-part system including an analyzer body (10), calibrant cartridge (14), and sensor cartridge (12). A modular calibrant cartridge (14) is insertable into the analyzer body (10), and contains all necessary calibrant fluids as well as a waste container. A modular sensor cartridge (12) having integral pump tubing (16) plugs into the analyzer body (10) for easy removal and replacement of the sensor elements. The analyzer body (10) internally has modular units including an electronics module, a display module, and a fluidics/printer module. The analyzer uses a single pump head (18) to aspirate blood only to a sensor array within the sensor cartridge (12). This action is accomplished by aspirating blood by rotating a peristaltic pump (18) in one direction during a first portion of an analysis cycle, and by reversing the pump (18) and flushing the blood from the sensor cartridge (12) with fluid pumped from the opposite direction during a second portion of an analysis cycle. Accordingly, blood contacts only a small portion of the analyzer mechanism, most of which is disposable. Because all valves are "downstream" from the single pump, no blood products pass through any valves. The analyzer fluid handling section is easily cleaned by removal of the sensor cartridge (12), yielding a single tube pathway. A short path length for blood travel permits using blood samples as small as 200 μ l. The analyzer is light and modular in design and is fully automatic.



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PORABLE MODULAR BLOOD ANALYZER WITH SIMPLIFIED
FLUID HANDLING SEQUENCE

BACKGROUND OF THE INVENTION

2. *Field of the Invention*

5 This invention relates to blood analyzers, and more particular to portable blood analyzers capable of analyzing multiple analytes.

3. *Description of Related Art*

Blood analyzers are medical instruments capable of analyzing one or more analytes, such as blood values for oxygen, carbon dioxide, pH, hematocrit, and electrolytes, such as 10 potassium, sodium, and calcium ions. Most prior art blood analyzers capable of measuring more than one analyte are complex, requiring specialized service skills and operator experience. Such multiple analyte blood analyzers have generally weighed in excess of 30 pounds, and have had sensor electrodes and plumbing (fluid path) that are complicated and require specialized knowledge to service. Many such blood analyzers 15 require tonometered gases in rigid or semi-rigid tanks to calibrate the sensors.

Prior blood analyzers have also often suffered from problems relating to clotting or blockage by proteinaceous materials which occlude fluid handling elements of the instrument. Analyzers which carry blood samples over long distances through multiple banks of electrodes are more susceptible to such problems. Also, blood elements tend to 20 obstruct traditional valving systems. When blood obstruction occurs in instrumentation, intensive disassembly and servicing has generally been required. Generally, blood analyzers having longer blood paths have more valves, and are generally complex and costly.

Accordingly, after noting the limitations of the above-described prior art, the inventors 25 of the present invention have devised a new blood analyzer that overcomes these problems.

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SUMMARY OF THE INVENTION

The present invention comprises a portable, modular blood analyzer capable of analyzing multiple blood values in an inexpensive, relatively simple, easy-to-use and easy-to-maintain instrument. In the preferred embodiment of the present invention, the invention

- 5 comprises a three-part system including an analyzer body, calibrant cartridge, and sensor cartridge. A modular calibrant cartridge is insertable into the analyzer body, and contains all necessary calibrant fluids as well as a waste container. A modular sensor cartridge having integral pump tubing plugs into the analyzer body for easy removal and replacement of the sensor elements. The analyzer body internally has modular units
- 10 comprising an electronics module, a display module, and a fluidics/printer module.

The inventive analyzer also uses a single pump head to aspirate blood only to a sensor array within the sensor cartridge, thus minimizing exposure of blood to internal valves and fluid handling circuits within the analyzer body. This action is accomplished by aspirating blood by rotating an peristaltic pump in one direction during a first portion of

- 15 an analysis cycle, and by reversing the pump and flushing the blood from the sensor cartridge with fluid pumped from the opposite direction during a second portion of an analysis cycle. Accordingly, blood contacts only a small portion of the analyzer mechanism, most of which (*i.e.*, the sensor cartridge) is disposable. Because all valves are "downstream" from the single pump, no blood products pass through any valves. The
- 20 analyzer fluid handling section is easily cleaned by removal of the disposable sensor cartridge, yielding a single tube pathway. A short path length for blood travel permits using blood samples as small as about 200 µl, and preferably less than about 150 µl.

The analyzer is light-weight and modular in design and is fully automatic. The analyzer can be serviced and operated by non-skilled or lesser skilled personnel, who can insert

- 25 and remove the low-cost sensor cartridge and calibrant cartridge without tools or special knowledge of the mechanism.

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The details of the preferred embodiment of the present invention are set forth in the accompanying drawings and the description below. Once the details of the invention are known, numerous additional innovations and changes will become obvious to one skilled in the art.

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BRIEF DESCRIPTION OF THE DRAWINGS

FIGURE 1 is a perspective view of the preferred embodiment of the blood analyzer of the present invention.

FIGURE 2 is a rear plan view of the preferred embodiment of the blood analyzer of the
5 present invention.

FIGURE 3 is a perspective view of the preferred embodiment of the blood analyzer of the present invention with the sensor cartridge and calibrant cartridge next to the analyzer body.

FIGURE 4 is an x-ray side view of the preferred embodiment of the blood analyzer of
10 the present invention.

FIGURE 5 is a schematic of the electrical and electronic connections of the preferred embodiment of the blood analyzer of the present invention.

FIGURE 6 is a block diagram of the fluid flow path of the preferred embodiment of the blood analyzer of the present invention.

15 FIGURE 7 is a flowchart of the fluid flow operation during calibration for the preferred embodiment of the blood analyzer of the present invention.

FIGURE 8 is a flowchart of the fluid flow operation during sampling for the preferred embodiment of the blood analyzer of the present invention.

Like reference numbers and designations in the various drawings indicate like elements.

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DETAILED DESCRIPTION OF THE INVENTION

Throughout this description, the preferred embodiment and examples shown should be considered as exemplars, rather than as limitations on the present invention.

FIGURE 1 is a perspective view of the preferred embodiment of the blood analyzer 10 of the present invention. FIGURE 2 is a rear plan view of the same analyzer 10. FIGURE 3 is a perspective view of the analyzer 10 of the present invention with a sensor cartridge 12 and calibrant cartridge 14 next to the body of the analyzer 10. FIGURE 4 is an x-ray side view of the blood analyzer 10.

The analyzer 10 includes a plug-in sensor cartridge 12 that provides sensors for measuring such blood characteristics as oxygen, carbon dioxide, pH, hematocrit, and electrolytes, such as potassium, sodium, and calcium ions. However, fewer or more analyte sensors can be included within the sensor cartridge 12. The sensor cartridge 12 preferable plugs in so that electrical contacts and plumbing connections are via "press-on" or "bayonet" type fittings without tools. In the preferred embodiment, a latch mechanism may be used to hold the removable sensor cartridge 12 in place. A loop of elastomeric tubing 16 attached to the sensor cartridge 12 is stretched to fit around a peristaltic pump head 18. (See also FIGURE 6). The sensor cartridge 12 and elastomeric tubing 16 are preferably made of transparent materials so that the flow of blood samples and fluids can be seen at all times, permitting visual detection of bubbles that can adversely affect operation of the analyzer 10. When attached to the analyzer 10, the sensor cartridge 12 is in fluid communication with the calibrant cartridge 14 and in signal communication with analyte determination circuitry within the analyzer (note that some electronics may be included within the sensor cartridge itself). Details of the construction and operation of a preferred sensor cartridge 12 are set forth in related patent applications (5) through (10) identified above under RELATED APPLICATIONS.

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The analyzer 10 includes a plug-in calibrant cartridge 14. The calibrant cartridge 14 preferably houses at least two flexible bags containing calibrant fluids (Calibrant A and Calibrant B), and an initially empty waste bag. The calibrant cartridge 14 preferable plugs in so that plumbing connections are via "press-on" or "bayonet" type fittings 15, 5 such as a Luer fitting, without tools. As shown in FIGURE 4, the fittings 15 are preferably at the bottom of the calibrant cartridge 14 to provide a gravity assist to calibrant fluid flow and to provide a very short fluid path for the overall system. In the preferred embodiment, a latch mechanism 15 (shown in FIGURE 2) in each removable calibrant cartridge 14 is used to positively engage the body of the analyzer 10, to ensure 10 a gas-tight fit of all fluid connections (necessary to maintain proper calibrant gas ratios) and to prevent inadvertent detachment of the calibrant cartridge 14. When both the calibrant cartridge 14 and the sensor cartridge 12 are installed within the analyzer 10, the sensor cartridge 12 is in fluid communication with each calibrant fluid container and the waste container in the calibrant cartridge 14 via internal plumbing within the analyzer 15 10. Details of the construction and operation of a preferred calibrant cartridge 14 are set forth in related patent applications (1) and (2) identified above under RELATED APPLICATIONS.

The preferred embodiment of the analyzer 10 includes a touch-screen display panel 20 for displaying instructions, indicating test results and messages, and providing an input 20 means for entering in data about calibrants, patients, accounting information, *etc.* The user interface for the display panel 20 is preferably menu or icon driven, thereby substantially reducing the amount of keyboard input required by a user. In the preferred embodiment, a removable media data storage device 22, such as a floppy disk drive, is provided to allow capturing of data generated by the analyzer 10 and to provide a 25 convenient means of reprogramming the internal electronics of the analyzer 10.

The preferred embodiment of the analyzer 10 includes a fluidics/printer module 24 that comprises the a fluidics module board 122 (shown in FIGURE 5), internal plumbing, valves, manifolds, *etc.* for routing fluids to and from the sensor cartridge 12 and calibrant

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cartridge 14, as well as a printer 25 (shown in FIGURE 5) hidden behind a face panel 26 that can be used to print out varied information, such as the results of a particular blood analysis. The printer may be, for example, a thermal dot matrix printer. Use of the printer is optional, since results of an analysis may be communicated by means of the display panel 20 or transmitted to another site. If necessary, the fluidics/printer module 24 can be removed and replaced as a unit. By locating the fluidics hardware and printer within a module, the time required to service the analyzer is substantially reduced.

A sample port stylus 30 (shown in FIGURE 6) is hidden behind a flip-up panel 32 to protect it from contamination and damage when not in use. A convenient carrying handle 10 34 is provided to lift the analyzer 10, which, in the preferred embodiment, weighs less than about 20 lbs. with a filled calibrant cartridge 14 and the sensor cartridge 12 in place. The analyzer 10 preferably has dimensions no greater than about 12"W × 12"D × 12"H for convenient handling and siting, such as at a nursing station or other point-of-care placement.

- 15 Referring to FIGURE 4, the rear bottom portion of the analyzer 10 includes a power supply and electronics bay 40 for housing a computer board. In the preferred embodiment, a battery backup unit is provided within the power supply and electronics bay 40 to provide power for a significant time (e.g., one hour) to the analyzer 10 in the event of a power failure. This feature is particularly important in a medical setting.
- 20 Referring to FIGURE 2, the back panel of the analyzer 10 preferably includes a power switch 42, power connector 44, fuse box 46, modem line-in and line-out connector 48, input/output port (e.g., an RS-232 serial port) 50, an auxiliary keyboard connecter 52, fan vent port 56, speaker grill 58, and display contrast adjustment 60. Other ports may be provided as desired, such as a parallel printer port, a local area network connector,
- 25 barcode reader port, etc.

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FIGURE 5 is a schematic of the electrical and electronic connections of the preferred embodiment of the blood analyzer 10 of the present invention. A main computer board 100 is coupled to an input/output expander board 102 and a bus expansion board 104. In the preferred embodiment, the bus expansion board 104 is coupled to a touch screen controller 106 which is in turn coupled to the touch screen 108. An optional fax/modem board 110 is provided for remote communication with the analyzer 10, which permits a variety of functions, such as remote diagnostics and per use billing. In the preferred embodiment, input/output expander board 102 is coupled in known fashion to a speaker 112, the display panel 20, the floppy drive 22, a printer 25, and the input/output port 50 5 and auxiliary keyboard connecter 52 on the back panel of the analyzer 10. A video port (e.g., a VGA standard port) 114 may be provided if desired for an auxiliary display.

Also coupled to the main computer board 100 is an input/output processor board 120, which is coupled to a fluidics module board 122, a sample switch 124, and a barcode reader 126. By monitoring the sample switch 124, the input/output processor board 120 15 detects when the sample port stylus 30 is positioned to receive a sample. The barcode reader 126 is used to enter barcoded data on new calibrant cartridges 14 and/or sensor cartridges 12.

The fluidics module 122 controls at least one valve 128 under command of the main computer board 100 via the input/output processor board 120, and receives and 20 conditions signals from one or more blood gas sensors 130 and /or one or more electrolyte sensors 132. Received signals from the fluidics module 122 are transmitted to the input/output processor board 120 and processed in the main computer board 100.

Power to all systems is provided in conventional fashion by a DC power supply 140 coupled to an AC fuse and power switch 142.

25 FIGURE 6 is a block diagram of the fluid flow path of the preferred embodiment of the blood analyzer of the present invention. The sample port stylus 30 is coupled via a short

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(preferably less than about 7 cm) inlet tube 200 (internal to the analyzer 10) to a first port 202 the sensor cartridge 12. The elastomeric tubing loop 16 attached to the sensor cartridge 12 is stretched as shown around the peristaltic pump head 18. In the preferred embodiment, the pump head 18 provides bidirectional rotary motion that moves fluid 5 through the tubing loop 16 in known fashion. However, other types of peristaltic pump motion may be used, so long as it is bidirectional (alternatively, two pump heads may be used, each unidirectional but pumping in different directions). Further, the pump head may be configured so that the tubing loop 16 need not be wrapped around the pump head 18 by having, for example, pinch rollers that engage the tubing loop 16 along the plane 10 formed by the tubing loop 16 (from either the front or the back).

The sensor cartridge 12 is attached through a second port 204 to bidirectional Valve 2, which is preferably an electrically actuated two-way valve. A first port of Valve 2 is coupled to a waste path 210 to a waste collector 212. Optionally, a backflow prevention valve 214 is provided to keep waste fluid from re-contacting Valve 2. The output of the 15 waste collector 212 may be directly coupled to a waste container using gravity flow. However, in the preferred embodiment, to keep all fluids contained and away from human contact, and to provide ease of use, a peristaltic waste pump head 216 is provided to actively pump waste fluid to a waste bag within the removable calibrant cartridge 14. In the preferred embodiment, the calibrant cartridge 14 plugs into the analyzer 10 via a 20 calibrant/waste manifold 218.

A second port of Valve 2 is coupled to bidirectional Valve 1 via a calibrant path 220. A first port of Valve 1 is coupled via tubing to Calibrant A within an attached calibrant cartridge 14. A second port of Valve 1 is coupled via tubing to Calibrant B within an attached calibrant cartridge 14.

25 When properly operated, three fluid paths are formed due to the settings of Valve 1 and Valve 2, and the direction of pumping by the pump head 18:

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- (1) from the sample port stylus 30 through the sensor cartridge 12 through Valve 2 to the waste path 210 and on to the waste collector 212;
- (2) from Calibrant A through Valve 1 through the calibrant path 220 through Valve 2 through the sensor cartridge 12 to the sample port stylus 30;
- 5 (3) from Calibrant B through Valve 1 through the calibrant path 220 through Valve 2 through the sensor cartridge 12 to the sample port stylus 30.

FIGURE 7 is a flowchart of the fluid flow operation during calibration for the preferred embodiment of the blood analyzer of the present invention. Under control of the main computer board 100, input/output processor board 120, and fluidics module board 122, 10 Valve 1 is switched to Calibrant A and Valve 2 is switched to the calibrant path 220 (STEP 700). In the illustrated embodiment, the pump head 18 is rotated counter-clockwise so as to draw Calibrant A fluid from the calibrant cartridge 14 and pump that fluid through the sensor cartridge 12 (STEP 702). The first point of a two-point calibration of the sensors within the sensor cartridge 12 is then conducted, in known fashion (STEP 704). After the first point of calibration is done, Valve 1 is switched to 15 Calibrant B (STEP 706). The pump head 18 is rotated counter-clockwise so as to draw Calibrant B fluid from the calibrant cartridge 14 and pump that fluid through the sensor cartridge 12 (STEP 708). The second point of a two-point calibration of the sensors within the sensor cartridge 12 is then conducted, in known fashion (STEP 710). A single-point calibration may be conducted in similar fashion, using only one of the calibrant fluids.

In all cases, the calibrant fluid exits the sensor cartridge 12 via the first port 202 of the sensor cartridge 12, and flows through the sample port stylus 30 to drain to the waste collector 212. A drain tube 222 may be provided to prevent splashing. As noted above, 25 the optional waste pump 216 may be used to pump the waste calibrant into a waste bag within the calibrant cartridge 14.

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FIGURE 8 is a flowchart of the fluid flow operation during sampling for the preferred embodiment of the blood analyzer of the present invention. The sample port stylus 30 is inserted into a container of sample fluid (e.g., blood in a vial) (STEP 800). Under control of the main computer board 100, input/output processor board 120, and fluidics module board 122, Valve 2 is switched to the waste path 210 (STEP 802). In the illustrated embodiment, the pump head 18 is rotated clockwise so as to draw a sample through the sample port stylus 30 and into the sensor cartridge 12 (STEP 804). The desired sample components may then be sensed within the sensor cartridge 12 (STEP 806). Any calibration fluid that had been in the sensor cartridge 12 (e.g., from prior flushing or 10 calibration) exits the sensor cartridge 12 via second port 204 and passes through Valve 2 to the waste path 210.

After a sample has been analyzed, Valve 2 is switched to the calibrant path 220 and Valve 1 is switched to a flushing calibrant (Calibrant B in this example) (STEP 808). The pump head 18 is rotated counter-clockwise so as to draw Calibrant B fluid from the 15 calibrant cartridge 14 and pump that fluid through the sensor cartridge 12, thereby flushing the sample out of the sensor cartridge 12. The waste fluid (sample and Calibrant B) exits the sensor cartridge 12 via the first port 202 of the sensor cartridge 12, and flows through the sample port stylus 30 to drain to the waste collector 212.

Importantly, the control system ensures that the whole undiluted blood sample is never 20 pumped past the pump head 18, and thus is never in contact with either Valve 2 or Valve 1.

In an alternative embodiment, Valve 1 can be eliminated by changing Valve 2 from a three-way valve as shown, to a four-way valve, and directly coupling Calibrant A and Calibrant B to Valve 1. Any other valving system that provides the three paths described 25 above can also be used, such as by using three two-way valves.

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As a result of this simple fluidics system, the invention minimizes exposure of internal valves and fluid handling circuits within the analyzer body to samples. Accordingly, blood contacts only a small portion of the analyzer mechanism, most of which (*i.e.*, the sensor cartridge) is disposable. Because all valves are "downstream" from the single 5 pump, no blood products pass through any valves. Only a single pump is required, thus reducing the cost of manufacture. The analyzer fluid handling section is easily cleaned by removal of the disposable sensor cartridge, yielding a single tube pathway. The short path length for blood through the sample port stylus 30 and inlet tube 200 permits using blood samples as small as about 200 μ l, and preferably less than about 150 μ l.

- 10 The control for the fluidics system is preferably accomplished via one or more control programs operating on the main computer board 100 and controlling the fluidics module board 122 through the input/output processor board 120. Program code is applied to input data to perform the functions described above and generate output information. The output information is applied to one or more output devices or actuators, as described 15 above.

Each program is preferably implemented in a high level procedural or object oriented programming language to communicate with the computer system. However, the programs can be implemented in assembly or machine language, if desired. In any case, the language may be a compiled or interpreted language.

- 20 Each such computer program is preferably stored on a storage media or device (*e.g.*, "flash" RAM, ROM, or magnetic diskette) readable by a general or special purpose programmable computer, for configuring and operating the computer when the storage media or device is read by the computer to perform the procedures described herein. The inventive system may also be considered to be implemented as a computer-readable 25 storage medium, configured with a computer program, where the storage medium so configured causes a computer to operate in a specific and predefined manner to perform the functions described herein.

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A number of embodiments of the present invention have been described. Nevertheless, it will be understood that various modifications may be made without departing from the spirit and scope of the invention. Accordingly, it is to be understood that the invention is not to be limited by the specific illustrated embodiment, but only by the scope of the
5 appended claims.

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CLAIMS

What is claimed is:

1. A portable, modular blood analyzer capable of analyzing at least one analyte value of a blood sample, comprising:
 - 5 (a) an analyzer body including at least one accessible pump head and analyte determination circuitry;
 - (b) a removable calibrant cartridge having at least one calibrant fluid container having calibrant fluid for performing at least one analysis of at least one analyte value of a blood sample, and having at least one waste container, the removable calibrant cartridge being configured to attach to the analyzer body without tools; and
 - (c) a removable sensor cartridge having integral pump tubing for peristaltic engagement with the pump head, the sensor cartridge including at least one sensor for performing at least one analysis of at least one analyte value of a blood sample, the removable sensor cartridge being configured to attach to the analyzer body without tools, and, when so attached, to be in fluid communication with each calibrant fluid container and the waste container and in signal communication with the analyte determination circuitry.
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- 15

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2. The blood analyzer of claim 1, further including, internal to the analyzer body, an electronics module embodying control circuitry for receiving input signals from the removable sensor cartridge, for generating at least one analysis of at least one analyte value of a blood sample, for outputting the results of each such analysis, and for controlling the operation of the blood analyzer.
5
3. The blood analyzer of claim 1, further including a display module attached to the analyzer body, for displaying results of each such analysis.
4. The blood analyzer of claim 1, further including a printer module internal to
10 the analyzer body, for printing results of each such analysis.
5. The blood analyzer of claim 1, wherein the blood analyzer with attached removable calibrant cartridge and removable sensor cartridge, weighs less than about 20 pounds.
6. The blood analyzer of claim 1, wherein the blood analyzer with attached
15 removable calibrant cartridge and removable sensor cartridge, measures less than about 12"W × 12"D × 12"H.
7. The blood analyzer of claim 1, wherein the calibrant cartridge includes a latching mechanism to maintain a gas-tight fit with the analyzer body when the analyzer body is attached to the analyzer body.

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8. A portable, modular blood analyzer capable of analyzing at least one analyte value of a blood sample, comprising:

- (a) an analyzer body including analyte determination circuitry;
- (b) a removable calibrant cartridge having at least one calibrant fluid container having calibrant fluid for performing at least one analysis of at least one analyte value of a blood sample, and having at least one waste container, the removable calibrant cartridge being configured to attach to the analyzer body without tools;
- (c) a removable sensor cartridge having integral pump tubing for engagement with a peristaltic pump mechanism, the sensor cartridge including at least one sensor for performing at least one analysis of at least one analyte value of a blood sample, the removable sensor cartridge being configured to attach to the analyzer body without tools, and, when so attached, to be in fluid communication with each calibrant fluid container and the waste container and in signal communication with the analyte determination circuitry;
- (d) at least one valve situated to alternatively couple the sensor cartridge to a waste port and to at least one calibrant fluid container within the calibrant cartridge;
- (e) a sample port, in fluid communication with the sensor cartridge, for drawing a blood sample into the sensor cartridge;
- (f) a bidirectional pumping mechanism having a pump head and positioned between the sensor cartridge and each valve, for engaging the pump tubing of the sensor cartridge, and for selectively pumping in a direction towards the waste port and in a direction towards the sample port;

wherein the blood analyzer is automatically operated to:

- (g) switch each valve to couple the sensor cartridge to the waste port;
- (h) actuate the bidirectional pumping mechanism to pump in a direction towards the waste port;

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- (i) draw a blood sample into the sensor cartridge through the sample port;
- (j) sense desired analyte values of the blood sample within the sensor cartridge;
- 5 (k) switch each valve to couple the sensor cartridge to one of the calibrant fluid containers within the calibrant cartridge;
- (l) reverse each pump to pump fluid from the calibrant fluid container in a direction towards the sample port, thereby flushing the blood sample from the sensor cartridge and sample port.

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9. The blood analyzer of claim 8, further including, internal to the analyzer body, an electronics module embodying control circuitry for receiving input signals from the removable sensor cartridge, for generating at least one analysis of at least one analyte value of a blood sample, for outputting the results of each such analysis, and for controlling the operation of the blood analyzer.
5
10. The blood analyzer of claim 8, further including a display module attached to the analyzer body, for displaying results of each such analysis.
11. The blood analyzer of claim 8, further including a printer module internal to
10 the analyzer body, for printing results of each such analysis.
12. The blood analyzer of claim 8, wherein the blood analyzer with attached removable calibrant cartridge and removable sensor cartridge, weighs less than about 20 pounds.
13. The blood analyzer of claim 8, wherein the blood analyzer with attached
15 removable calibrant cartridge and removable sensor cartridge, measures less than about 12"W × 12"D × 12"H.
14. The blood analyzer of claim 8, wherein the calibrant cartridge includes a latching mechanism to maintain a gas-tight fit with the analyzer body when the analyzer body is attached to the analyzer body.

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15. A method of processing a sample within a blood analyzer, comprising the steps of:

- (a) switching at least one valve to couple a sensor cartridge to a waste port;
- 5 (b) actuating at least one pump, positioned between the sensor cartridge and each valve, to pump in a direction towards the waste port;
- (c) drawing a blood sample into the sensor cartridge blood analyzer via a sample port;
- (d) sensing desired components of the blood sample within the sensor cartridge;
- 10 (e) switching each valve to couple the sensor cartridge to a fluid source;
- (f) reversing each pump to pump fluid from the fluid source in a direction towards the sample port, thereby flushing the blood sample from the sensor cartridge and sample port with fluid.

15 16. The method of claim 15, wherein substantially no amount of the blood sample is pumped past any pump.

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17. A computer program, residing on a computer-readable medium, to implement a method of processing a sample within a blood analyzer, comprising instructions for causing a computer to:

5 (a) switch at least one valve to couple a sensor cartridge to a waste port;

 (b) actuate at least one pump, positioned between the sensor cartridge and each valve, to pump in a direction towards the waste port;

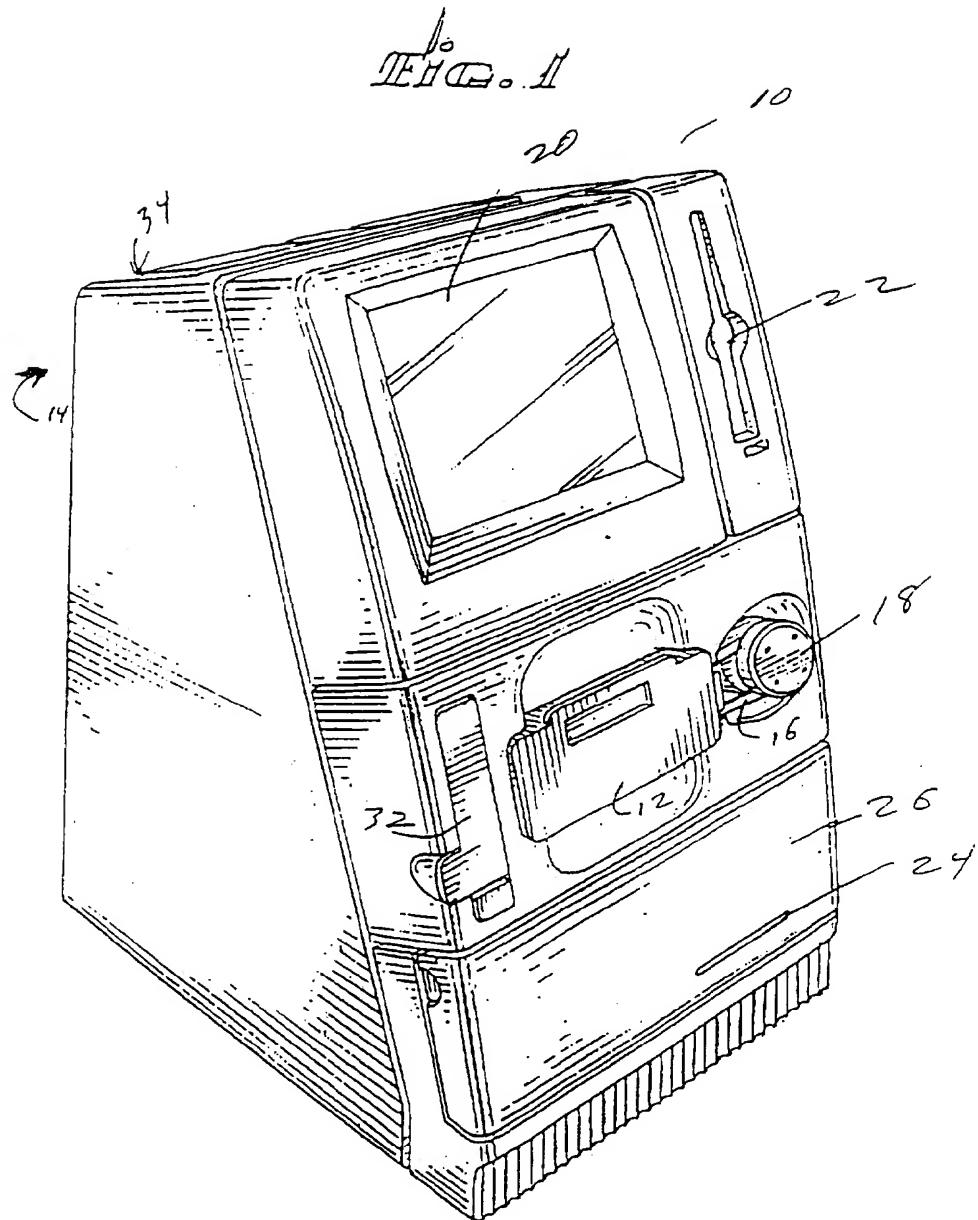
 (c) draw a blood sample into the sensor cartridge blood analyzer via a sample port;

 (d) sense desired components of the blood sample within the sensor cartridge;

10 (e) switch each valve to couple the sensor cartridge to a fluid source;

 (f) reverse each pump to pump fluid from the fluid source in a direction towards the sample port, thereby flushing the blood sample from the sensor cartridge and sample port with fluid.

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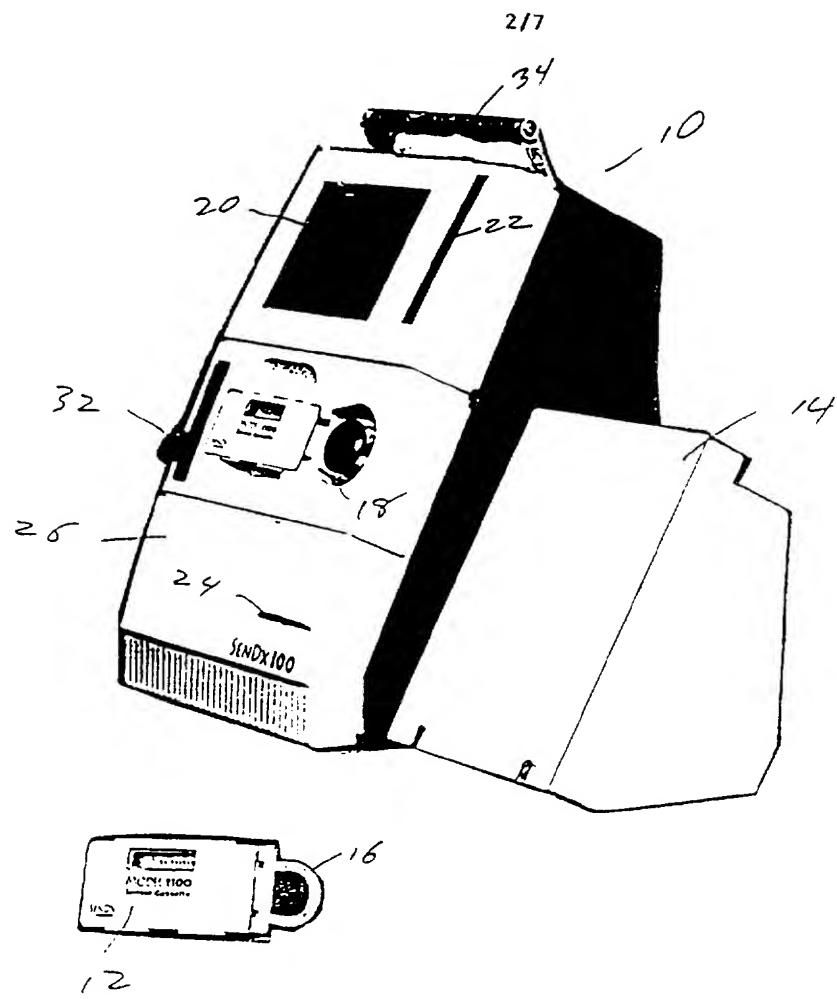
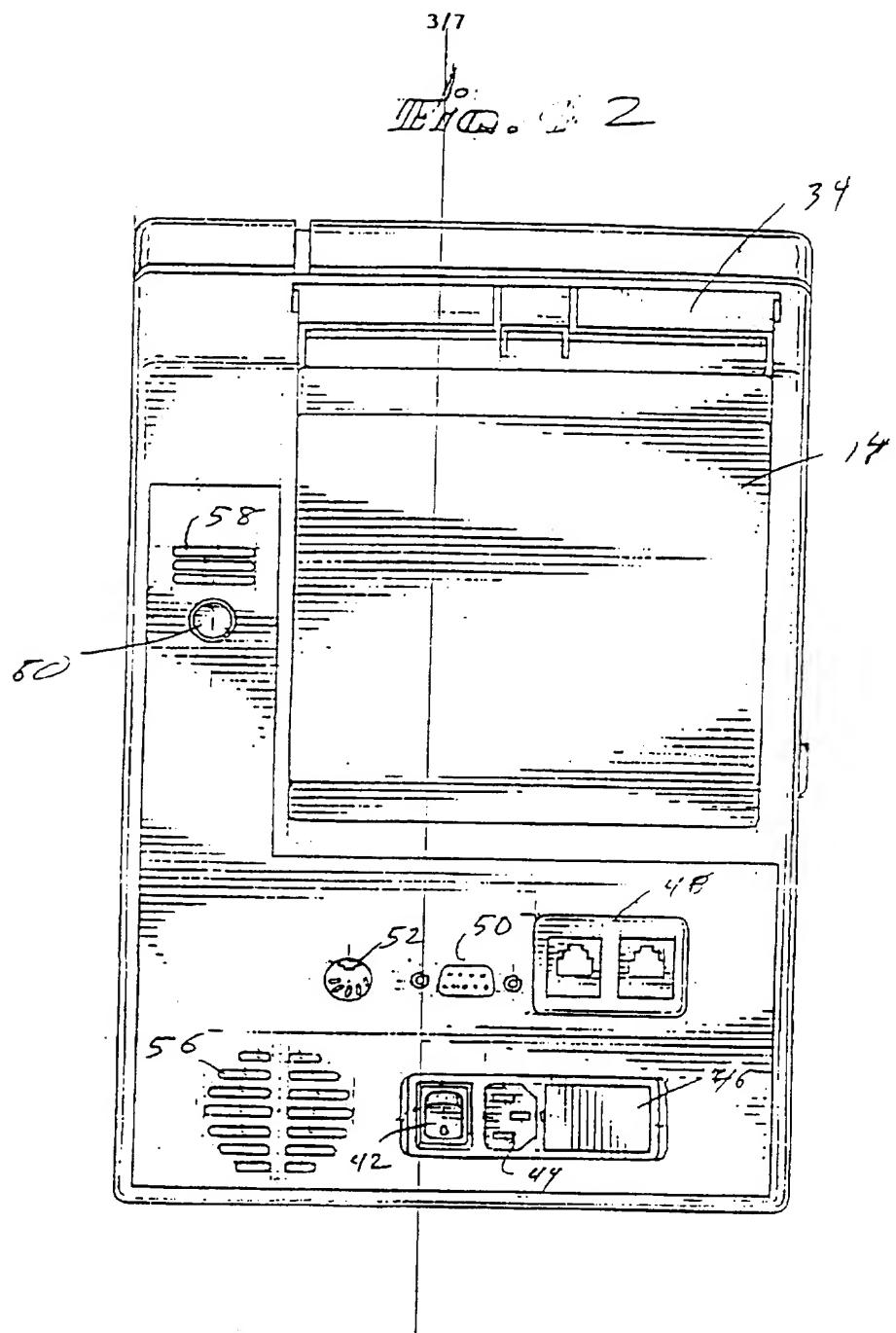
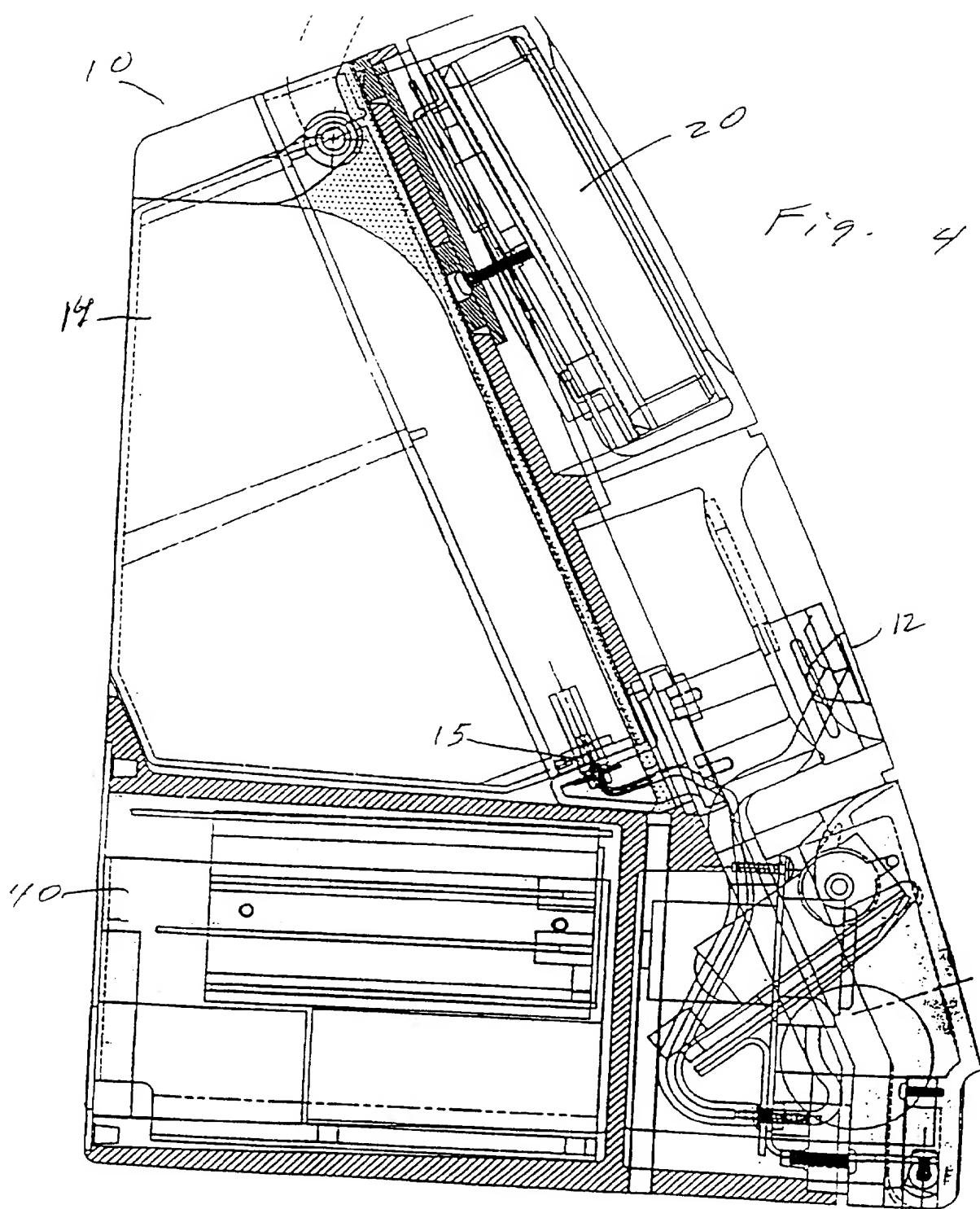
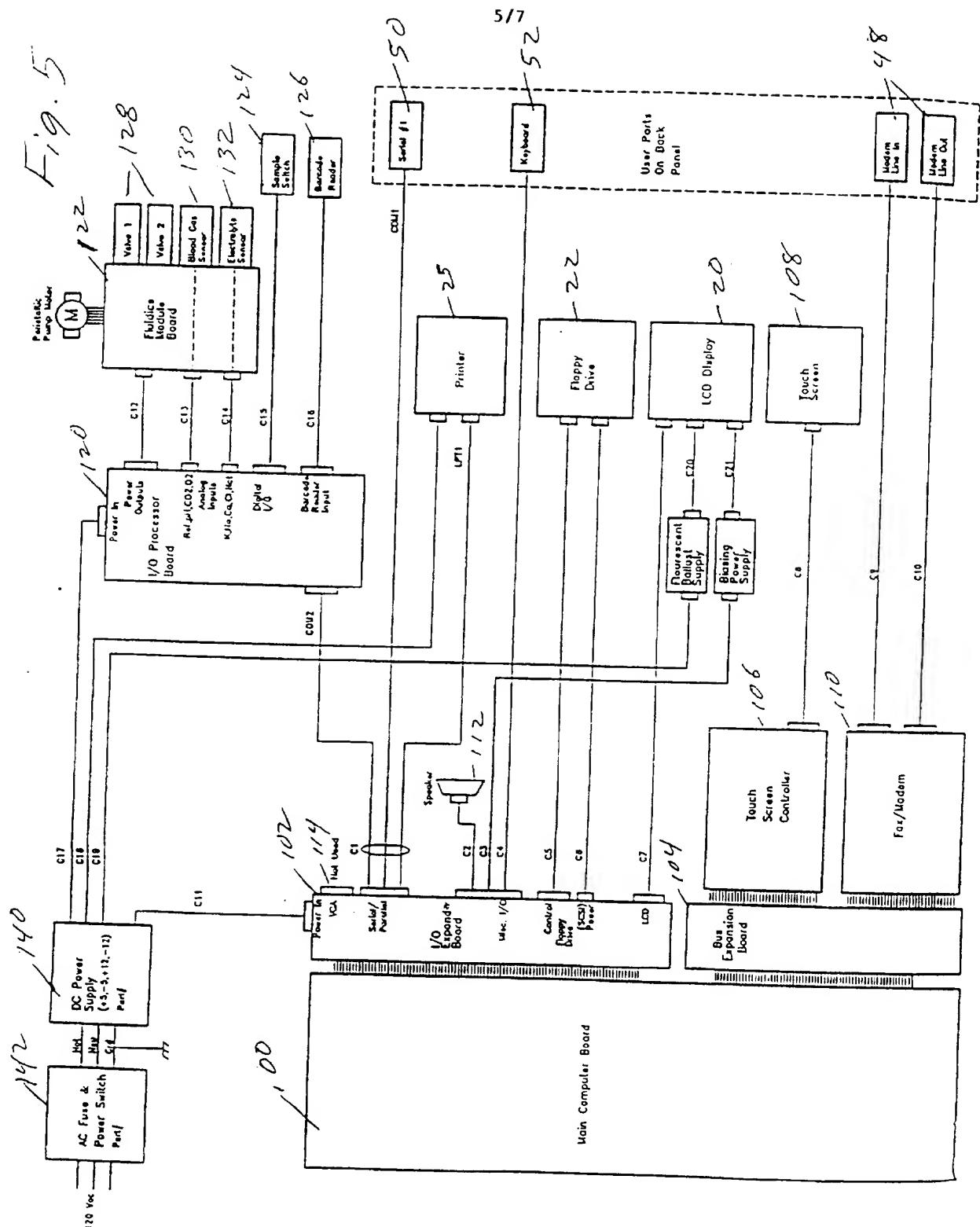


Fig. 3

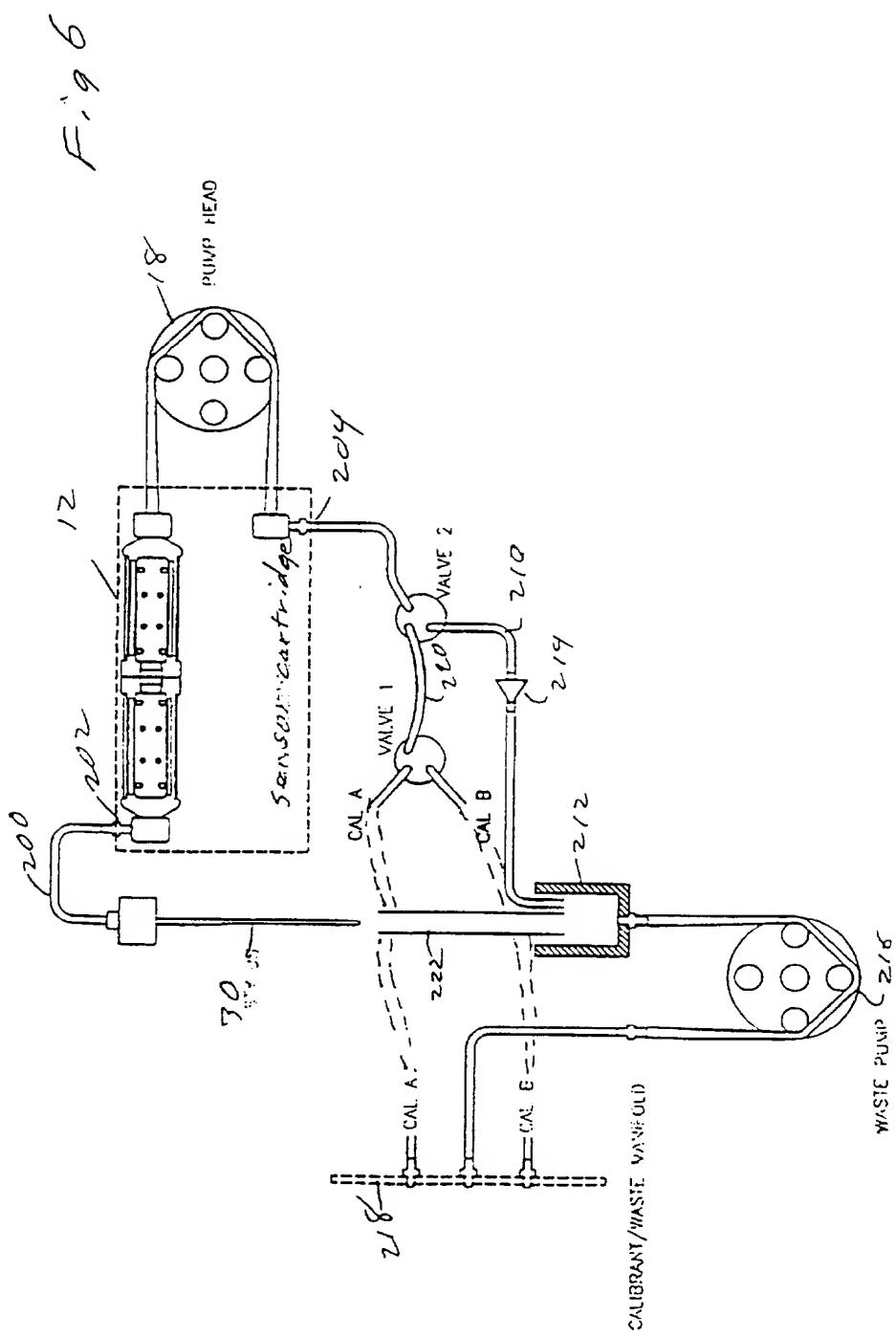


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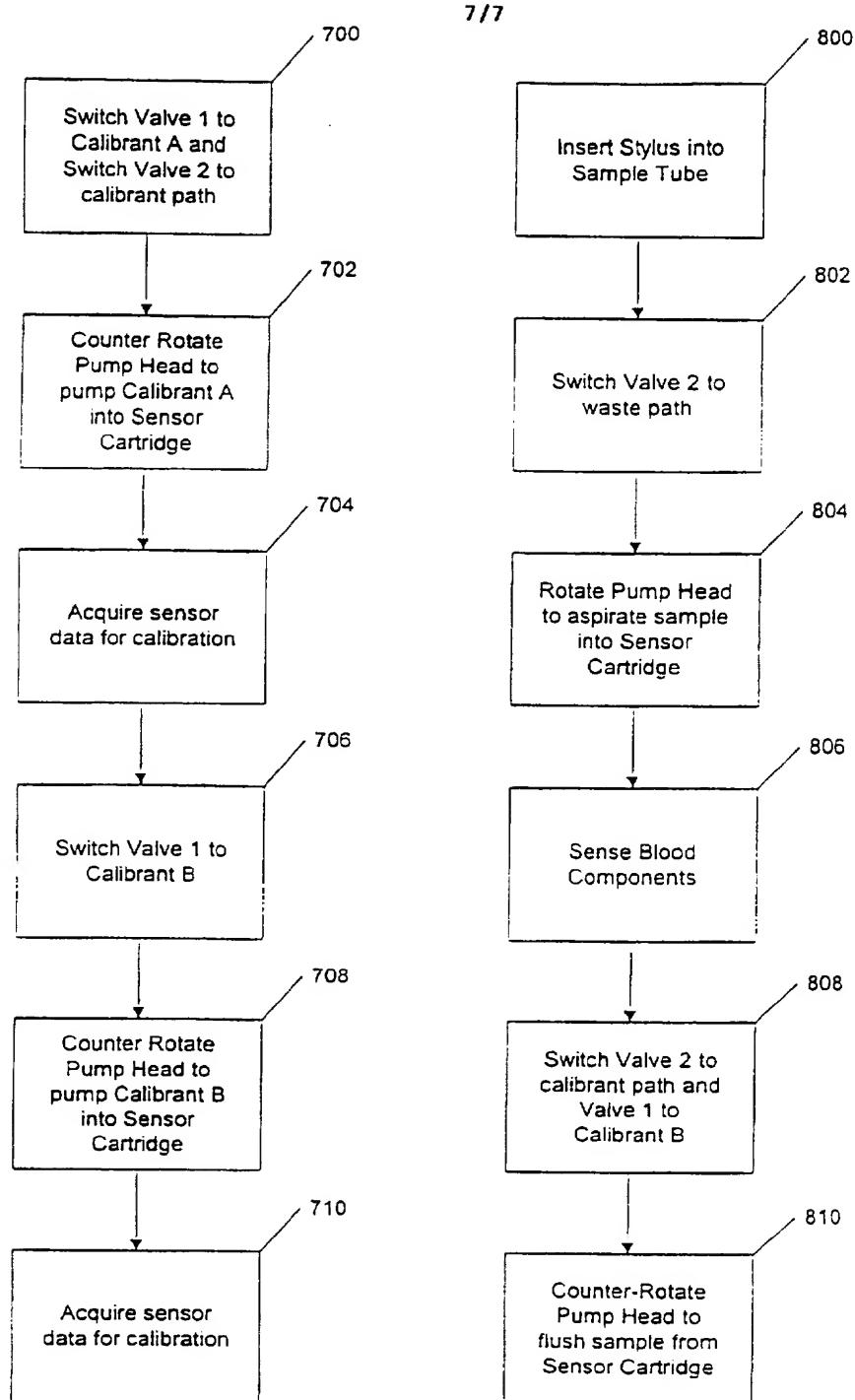


FIG. 7

FIG. 8

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US97/08737

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) :G01N 35/10

US CL :422/58, 61, 63, 81, 100, 104; 436/43,46,52,174, 180, 183; 364,497

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 422/58, 61, 63, 81, 100, 104; 436/43,46,52,174, 180, 183; 364,497

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US 4,871,439 A (ENZER ET AL.) 03 OCTOBER 1989, FIGURES 1 AND 2.	1-17
Y	US 5,284,568 A (PACE ET AL.) 08 FEBRUARY 1994, figures 1-3, column 1, line 50 to column 2, line 52.	1-17
A	US 5004583 A (GURUSWAMY ET AL.) 02 April 1991, figures 1 and 3.	1-17
A, P	US 5519635 A (MIYAKI ET AL.) 21 May 1996, figures 1-3.	1-17

Further documents are listed in the continuation of Box C. See patent family annex.

* Special categories of cited documents:	"T"	later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"A"		document defining the general state of the art which is not considered to be of particular relevance
"E"	"X"	earlier document published on or after the international filing date
"L"		document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
"O"	"Y"	document referring to an oral disclosure, use, exhibition or other means
"P"	"&"	document published prior to the international filing date but later than the priority date claimed

Date of the actual completion of the international search

17 AUGUST 1997

Date of mailing of the international search report

11 SEP 1997

Name and mailing address of the ISA/US
Commissioner of Patents and Trademarks
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Washington, D.C. 20231

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INTERNATIONAL SEARCH REPORTInternational application No.
PCT/US97/08737**Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)**

This international report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. Claims Nos.: because they relate to subject matter not required to be searched by this Authority, namely:

2. Claims Nos.: because they relate to parts of the international application that do not comply with the prescribed requirements to such an extent that no meaningful international search can be carried out, specifically:

3. Claims Nos.: because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

Please See Extra Sheet.

1. As all required additional search fees were timely paid by the applicant, this international search report covers all searchable claims.
2. As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. As only some of the required additional search fees were timely paid by the applicant, this international search report covers only those claims for which fees were paid, specifically claims Nos.:

4. No required additional search fees were timely paid by the applicant. Consequently, this international search report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

The additional search fees were accompanied by the applicant's protest.

No protest accompanied the payment of additional search fees.

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US97/08737

BOX II. OBSERVATIONS WHERE UNITY OF INVENTION WAS LACKING
This ISA found multiple inventions as follows:

This application contains the following inventions or groups of inventions which are not so linked as to form a single inventive concept under PCT Rule 13.1. In order for all inventions to be searched, the appropriate additional search fees must be paid.

Group I, claim(s) 1-16, drawn to a portable blood analyzer and a method of processing a sample.
Group II, claim(s) 17, drawn to a computer program in a blood analyzer.

The inventions listed as Groups I and II do not relate to a single inventive concept under PCT Rule 13.1 because, under PCT Rule 13.2, they lack the same or corresponding special technical features for the following reasons: the claims of groups I and II are drawn to distinct inventions which are not linked so as to form a single general inventive concept. Group I is drawn to a blood analyzer while group II is drawn to a computer program. PCT Rules 13.1 and 13.2 do not provide for multiple distinct inventions.